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Cover Page Footnote

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Nanomaterial-based adsorbents and optical sensors for illicit drug analysis

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Abstract

The abuse of illicit drugs has been prevalent in recent years and is associated with crime and public health issues. To strengthen public security and fortify public health services with respect to the increasing severity of drug abuse, academic and government institutes have been devoted to constructing relative analytical methods for illicit drugs. To date, the development of sensors has been greatly emphasized due to their features of high sensitivity, prompt detection and flexible manipulation; thus, sensors can serve as alternatives to conventional sophisticated instruments. Recently, the use of nanomaterials has inspired the development of a series of innovative sample pretreatment and detection strategies in the field of analytical chemistry. Herein, this review elaborated the application of nanomaterials in analytical methods, including sample pretreatments, colorimetric sensors and fluorescent sensors. The utilization of nanomaterials in the analytical field provides novel perspectives for the development of detection platforms and facilitates the monitoring of illicit drugs in diverse complex matrices.

Keywords: Nanomaterial, Adsorbents, Colorimetric sensors, Fluorescent sensors, Illicit drugs

1. Introduction

The prevalence of drug abuse has become a severe public health issue and a serious criminal issue worldwide in recent years. Illicit drugs accompanied by addiction, organ dysfunction and fatality at high doses are categorized on the basis of their traits as depressants, stimulants, narcotics or hallucinogens [1]. The abuse of these drugs can gradually deteriorate the mental or physical condition of users. The United Nations Office on Drugs and Crime reported that an enormous number of individuals, up to 188 million, have used cannabis as a hallucinogen at least once. Stimulants, such as cocaine, amphetamine and methamphetamine, are the second most abused drugs, with 68 million users. Among

them, cocaine accounted for 18 million users in 2017. Furthermore, 50 million individuals worldwide had taken up opioids in 2017 [2]. In Taiwan, the data according to the Analytic Laboratory Drug Abuse Report System from 1999-2011 also showed that methamphetamine was the most widely abused drugs [3]. According to the annual statistic of abusing drugs in 2018 in Taiwan, 36,746 individuals who were influenced by illicit drugs were reported, which presented an increasing trend from 2016 to 2018. Moreover, the cases of polypharmacy were also determined to be up to 73%. Among these cases, the dual combination of illicit drugs accounts for 81.2% of multiple drug abuse. Methamphetamine and 3, 4-methylenedioxy-methamphetamine (MDMA) were the most prevalent drugs used in dual combination.

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Other illicit drugs can be also found in multiple drug abuse, such as ketamine, norketamine, morphine and codeine [4]. To efficiently control the extending prevalence of drug abuse, the government in Taiwan also legislated cut-off levels of illicit drugs in human urine which presented in Table 1 [5,6]. Regulations in EU and USA corresponding to that in Taiwan are also listed in the table [7–9].

The main test methods for determining the presence of illicit drugs in medical and government institutions include liquid chromatography coupled with (tandem) mass spectrometry (LC-MS or LC-MS/MS) [10,11], gas chromatography coupled with mass spectrometry (GC-MS) [12] and immunoassays [13], which are commercially available and widely utilized for monitoring the levels of illicit drugs. In recent decades, the nanomaterial-based analytical techniques have become a novel trend in illicit drug analysis. Nanomaterials possess unique characteristics such as high surface area, ease of modification, which can perform diverse application, such as sample pretreatment and biosensor establishment, so as to facilitate the monitoring illicit drugs.

To monitor the levels of illicit drugs efficiently, the sample pretreatment procedure is a crucial factor to obtain ideal performance on detection. Nevertheless, the elimination of interferences from complex matrices may be challenged for the detection of illicit drugs because the detection usually implemented in human body fluids (blood, urine, hair and saliva ...), foods and beverages which compose of varied compounds.

Sample pretreatment coupled with nanometer-sized magnetic nanoparticles (MNPs), can provide faster phase separation by applying an external magnetic field and be easy to reuse. MNPs also can be utilized to

generate a high selectivity, facile extraction procedure, less reagent consumption compared to conventional sample pretreatment methods.

In addition to sample pretreatment methods, nanomaterials can also be applied as signal reporters that provide rapid and sensitive detection. Nanomaterial-based optical sensor systems can be categorized into colorimetric and fluorescent sensor systems. In colorimetric methods, noble metal nanoparticles, namely gold and silver, were universally utilized nanomaterials attributed to their unique optical property of surface plasmon resonance (SPR) [14,15]. The phenomenon of SPR facilitates the visual observation of the color change of nanomaterials when the analyte is added into the detection system. Regarding fluorescent methods, nanomaterials were utilized to develop a versatile detection strategy. These kinds of nanomaterials, such as nanoclusters (NCs), quantum dots (QDs), carbon dots (CDs) and upconversion nanoparticles (UCNPs), possess the trait of tunable luminescent emission, which can be substituted for conventional fluorescent indicators such as fluorescein (FAM), cyanine 3 (Cy3), carboxytetramethylrhodamine (TAMRA), carboxy-X-rhodamine (ROX), etc [16–19].

Attributed to the development of novel sensors, further evolution has also implemented a series of rapid diagnostic strategies for illicit drugs in combination with nanomaterials. This review mainly emphasizes the analytical techniques among nanomaterial-based adsorbents, nanomaterial-based colorimetric sensor systems and fluorescent sensors for the detection of illicit drugs.

2. Surface functionalized MNPs

Magnetic solid-phase extraction (MSPE) was first established in 1999 by Šafařčková et al. using

Table 1. Regulations of cut-off levels of illicit drugs in Taiwan, EU and USA.

	Taiwan (TFDA ¹)	EU (EMCDDA ²)		USA (HHS ³)	
	Urine (ng/mL)	Whole blood (ng/mL)	Oral fluid (ng/mL)	Urine (ng/mL)	Oral fluid (ng/mL)
Benzodiazepines	100	140 (Diazepam)	5 (Diazepam)	-	-
Amphetamine	500	20	360	250	25
Methamphetamine	500	20	410	250	25
MDMA	500	20	270	250	25
Morphine	300	10	95	2000	15
Codeine	300	10	94	2000	15
Cocaine	-	10	170	-	8
Benzoylcegonine	150	50	95	100	8
Ketamine	100	-	-	-	-
Norketamine	100	-	-	-	-
THC	15	1.0	27	15	2

Abbreviation: ¹ TFDA: Food and Drug Administration (Taiwan), ² EMCDDA: European Monitoring Centre for Drugs and Drug Addiction, ³ HHS: United States Department of Health and Human Services.

magnetic charcoal as an adsorbent [20]. MSPE is a novel technique that accomplishes extraction by the interaction between the functional group on the surface-modified magnetic material as the adsorbent and the analytes. Compared to conventional magnetic beads, nanometer-sized magnetic particles possess the properties of superparamagnetism, better dispersibility and higher surface area, which enhance the extraction efficiency [21]. In order to overcome the problems, such as complex matrices and time-consuming sample preparation, techniques on the basis of surface functionalized MNPs were developed to extract illicit drugs. Previous studies are summarized in Table 2 which presented extraction condition corresponding to each adsorbent in illicit drugs analysis.

2.1. Small organic molecules

The magnetic core of magnetic nanoparticles (MNPs) is mainly composed of iron, nickel, cobalt and their oxides. In conventional MNPs, small organic molecules were used to modify iron oxide MNPs, including carbon [22,23], methacrylic acid-3-(trimethoxysilyl) propyl ester (MPS) [24,25], which influences the ability of the adsorbent to capture illicit drugs such as methamphetamine [13,23], cocaine [24] and morphine [25] in urine or hair samples. The interaction between analytes and surface-modified magnetic nanoparticles was implemented by van der Waals forces, π - π stacking interactions, and hydrophobic or electrostatic interactions.

Boojaria et al. synthesized MPS-modified MNPs for extracting morphine from human hair. The pretreated 50 mg of hair sample was rinsed with ethanol and the solution was subsequently diluted with deionized water. After that, morphine was spiked into the treated hair solution. The recovery of morphine in hair solution by using MPS-modified MNPs was obtained to be 87.62%. Moreover, an enrichment factor of 208 was acquired by this method, which enhanced the detection sensitivity up to 0.1 ng/mL as the limit of detection (LOD) by HPLC-UV [25].

2.2. Polymer

The surface of fabricated MNPs from polymer are better than small molecules. It is found to have significant advantages, such as high stability in suspension. Haeri et al. established a biodispersible liquid-liquid microextraction (bio-DLLME) based on polypyrrole-coated iron oxide nanoparticles for methamphetamine extraction in urine [26]. The urine sample was first treated with polypyrrole-coated iron oxide nanoparticles, and the desorption

solution containing methamphetamine was further extracted by a rhamnolipid biosurfactant. The LOD was measured to be 0.33 ng/mL by HPLC-UV and an enrichment factor of 310 within 2 min of extraction time. In addition, carbon nanotubes (CNTs) [27,28] and graphene oxide (GO) [29,30] were also utilized as composites with iron oxide MNPs. CNTs and GO provide π - π stacking interactions and chelation sites for hydrogen bonds, respectively, to aromatic compounds such as methamphetamine, cocaine, ketamine, codeine and morphine [27–30]. The MSPE method, based on a magnetite/rGO/silver nanocomposite, was utilized for the extraction of codeine and morphine. The nanomaterials with high surface areas, suitable chemical surfaces and functional groups as adsorbed sites provided superior enrichment factors for analytes up to 1000 with a 15 min extraction time. The enrichment factor of the novel MSPE method is much higher than that obtained by conventional DLLME in the range of 63–85 [29].

2.3. Aptamer and antibody

The utilization of specific ligand, namely aptamer and antibody, as the extraction agent for illicit drugs provide specificity on sample pretreatment procedure. This kind of ligand can capture certain target from complex matrix and avoid interferences during detection. Aptamers, short single-strand DNA or RNA, can recognize analytes and increase the specificity of the extraction procedure. They are easy to obtain and more stable with respect to biodegradation. Du et al. developed a colorimetric sensor system for detecting cocaine [31]. Cocaine aptamers were modified on amine-functionalized MNPs and another cocaine aptamer with hemin-G-quadruplex hydrides with cocaine aptamer-modified MNPs when cocaine was present simultaneously. The aptasensor can capture the cocaine within a complex matrix by aptamer-modified MNPs in an external magnetic field. Hemin-G-quadruplex can catalyze the 3,3',5,5'-tetramethylbenzidine sulfate (TMB)-hydrogen peroxide system to trigger the color change of TMB from colorless to yellow. Using the aptasensor mechanism, cocaine can be quantified according to the TMB color change. In addition to aptamers, antibodies also have a high affinity for selective targets. When antibody-modified MNPs are prepared, amphetamine and methamphetamine can be purified from urine samples and analyzed by matrix-assisted laser desorption ionization time-of-flight mass spectrometer (MALDI-TOF MS) analysis [32]. Compared with other methods using surface functionalized MNPs, only 20–25 μ L sample and

Table 2. Various magnetic nanomaterial-based adsorbents for analysis of illicit drugs.

Surface functionalized MNPs	Sample volume	Adsorbent amount	Extraction time	Desorption time	Analytical Instrument	Enrichment factor	Sample	Limit of detection	Ref.
Small organic molecules									
Carbon	5 mL	40 mg	2 min	5 min	HPLC-UV	-	Urine	20 ng/mL for methamphetamine	[22]
Carbon	6 mL	15-mm iron wire	10 min	5 min	HPLC-UV	-	Urine	5 ng/mL for amphetamine	[23]
SMPS@PLS ¹	1 mL	10 mg	21 min	10 min	HPLC-MS	-	Urine	6 ng/mL for methamphetamine 0.09 ng/mL for benzoylecgonine 0.26 ng/mL for benzoynorecgonine 1.15 ng/mL for cocaethylene 0.92 ng/mL for cocaine 1.1 ng/mL for ecgonine 0.13 ng/mL for m-hydroxybenzoylecgonine 0.65 ng/mL for norcocaethylene 0.20 ng/mL for norcocaine 0.1 ng/mL for morphine	[24]
MPS ²	50 mg	15 mg	20 min	10 min	HPLC-UV	208.69	Hair	0.1 ng/mL for morphine	[25]
Polymer									
polypyrrole		30 mg	2 min	1 min	HPLC-UV	310	Urine	0.33 ng/mL for methamphetamine	[26]
o-MWNTs ³	4 mL	15 mg	10 min	10 min	GC-MS	-	Blood Urine	44 pg/mL for methamphetamine 24 pg/mL for ketamine	[27]
CNTs	500 µL	9 mg	2 min	2 min	GC-MS	-	Breast milk	1.5 ng/mL for benzoylecgonine 1.6 ng/mL for cocaine	[28]
rGO/AgNC ⁴	2 mL	100 mg	15 min	-	HPLC-UV	1000	Blood Urine	2.1 pg/mL for codeine 1.8 pg/mL for morphine	[29]
MNGO ⁵	10 mL	40 mg	25 min	15 min	HPLC-UV	168	Urine	30 ng/mL for methamphetamine	[30]
Aptamer									
5'-HS(CH ₂) ₆ -TTTTGGGA GTCAAGAACGAA-3'	25 µL	0.05 mg	40 min	-	UV	-	Plasma Serum Urine	15 ng/mL for cocaine	[31]
Antibody									
amphetamine antibody methamphetamine antibody	20 µL	0.01 mg	10 min	10 min	MALDI-TOF MS		Urine	1.87 ng/mL for amphetamine 3.75 ng/mL for methamphetamine	[32]

Abbreviation: ¹ SMPS@PLS: SiO₂ and methacrylic acid-3-(trimethoxysilyl) propyl ester-divinyl benzene and vinyl pyrrolidone core-shell, ² MPS: methacrylic acid-3-(trimethoxysilyl) propyl ester, ³ o-MWNTs: acid-oxidized multi-walled carbon-nanotubes, ⁴ rGO/AgNC: reduced graphene oxide/silver nanocomposite, ⁵ MNGO: magnetic nano graphene oxide.

0.01–0.05 mg adsorbent were needed when using aptamers or antibodies modified MNPs in illicit drug analysis. The ligand as the adsorbent with magnetic materials can be flexibly selected according to the target analytes by different synthesis protocols. Moreover, the cooperation of the aptamer and antibody provide the specificity of extraction, less sample and adsorbent consuming which also possesses a greater tendency to eliminate interference from the complex matrix.

In summary, magnetic nanomaterials-based adsorbents provide facile and flexible modification which can utilize to capture diverse illicit drugs. According to the efficiency of eliminating sample interferences integrated in Table 2, a large sample volume in the range of milliliter can be extracted and eluted with a small amount of solvent in few microliter. External magnetic field play an important role on capturing magnetic adsorbent binding with analyte so as to eliminate the sample matrix. The sample pretreatment by nanomaterials achieves not only effective separation of analyte from complex matrices but also pre-concentration of sample solution for signal amplification. In addition, the reusability of nanomaterials-based adsorbents was potentially available which was indicated in several literatures, such as five times-reused divinyl benzene and vinyl pyrrolidone functionalized silanized MNPs with acceptable recovery above 76.9% [24] and eighty continuous adsorption-desorption cycles for magnetite/rGO/silver nanocomposite without losing substantial extraction efficiency [29]. In the part of detection sensitivity, several analytical methods coupled with magnetic nanomaterials-based adsorbents can obtained LODs from 0.0018 to 20 ng/mL by HPLC-UV. Those obtained detection limits were close to LODs measured by MS system from 0.001 to 6 ng/mL with conventional LLE or SPE [22,26,29]. It means the sample pretreatment can effectively improve not only the efficiency of eliminating interferences from complex matrices but also enhance the sensitivity.

3. Nanomaterial-based colorimetric sensors

Colorimetric sensors are typically used in conjunction with nanoparticles due to their unique optical properties, surface dielectric environment and catalytic activity. AuNPs are one of the most iconic nanomaterials and have been widely applied in the establishment of colorimetric sensors due to their air stability and visible spectrum owing to d-d band transitions [14]. The color change of different sizes of AuNPs can be observed via the influence on the plasmon oscillation while irradiating by light,

namely, surface plasmon resonance (SPR) [33]. The colorimetric sensing systems developed to analyze illicit drugs were mainly small organic molecules-based AuNP sensors and aptamer-based AuNP sensors.

3.1. Small organic molecules-based AuNP sensors

Many sensors functioning on the basis of ligand interaction or ligand exchange have been established for the detection of illicit drugs that possess functional groups that are prone to interact with the ligand on the surface of AuNPs. The mechanism of citrate-capped AuNPs for the detection of abused drugs can be divided into ligand exchange on the surface of AuNPs [34] or ligand interaction between citrate and the analyte [35,36]. The ligand exchange process can be performed due to the weak surface-bound citrate as the ionic stabilization agent for the AuNPs [37]. Consequently, the molecules with stronger affinity to AuNPs can competitively displace the binding sites of citrate to AuNPs. In ligand exchange, Lodha et al. developed a biosensor for the detection of codeine sulfate in bone, bone marrow and soil [34]. Codeine sulfate can displace the weakly bound citrate on the surface of AuNPs via ligand exchange and further coordinate with the surface of AuNPs by multiple binding sites, such as sulfate groups and oxygen hybrid rings. The aggregation of AuNPs can be observed in the presence of codeine sulfate as the bridge between the AuNPs. The LOD for codeine sulfate was 0.6 µg/mL by a digital camera of a mobile phone [34]. The other mechanism for the citrate-capped AuNPs relies on the direct interaction between citrate and the analyte by the cross-linking process. A colorimetric sensor array was established for the detection of opioid analogs (codeine, methadone, morphine, noroxycodone, oxycodone, thebaine and tramadol) in urine [35]. The opioids possess many hydrogen bond donor/acceptor sites, including hydroxyl, methoxy and furan-like oxygen hybrid rings, which provide the link between citrate and opioids to induce the aggregation of AuNPs. Consequently, the LOD of noroxycodone was 6.7 µg/mL, and others were as low as 0.29 µg/mL [35]. A similar biosensor was established by Bahram et al. for the detection of morphine, and the LOD was 0.15 µg/mL in serum and urine samples [36].

Previous studies have demonstrated that electron-rich nitrogen-containing ligands possess high affinity for the surface of AuNPs [38], and melamine, as a nitrogen-containing ligand, has been widely applied in versatile detection strategies [39]. Lodha et al. fabricated a sensor for the detection of

clonazepam in blood, bone and bone marrow samples based on the aggregation of AuNPs by the interaction between melamine and clonazepam, which brings AuNPs closer to each other. An LOD of 0.28 ng/mL can be obtained by evaluating the absorption ratio ($A_{636\text{ nm}}/A_{552\text{ nm}}$) [40]. A similar mechanism of melamine-modified AuNPs was also applied to quantify the content of codeine and morphine in human serum and urine samples, and the LODs of morphine and codeine were 4.9 ng/mL and 2.7 ng/mL, respectively [41]. The incubation time of these colorimetric sensors were less than 10 min.

3.2. Aptamer-based AuNP sensors

The mechanism of colorimetric biosensors on the basis of aptamers (or oligonucleotides) for the detection of targets with high selectivity mainly depends on the unique property of the binding interaction between aptamers and analytes. Once the analyte is present in the detection system, the aptamer can form a complex with the analyte, and this phenomenon produces a conformational change on an aptamer that fails to perform hybridization or electrostatic interactions with other substances, such as complementary DNA or AuNPs [42].

In the case of oligonucleotide-assisted aggregation, the color change attributed to the aggregation of AuNPs depends on the distance between the AuNPs [43]. Liu et al. designed 3'-thio-modified DNA and 5'-thio-modified DNA immobilized on AuNPs (13 nm), respectively. In the absence of cocaine, 3'-thio-modified DNA and 5'-thio-modified DNA were assembled with linker DNA and a cocaine aptamer. A passive aggregation of AuNPs was observed by the color change of AuNPs from red to purple due to the redshift of the SPR wavelength. Once cocaine is present, the aptamer interacts with the cocaine, and the 5'-thio-modified DNA cannot complement the linker DNA. A red color was still observed because the distance between the AuNPs did not shorten [44]. In addition, the mechanism of oligonucleotide-assisted aggregation was also applied to detect cocaine in latent fingerprints (LFPs) by nanoplasmonic imaging [45]. Cocaine aptamers with two single-strand DNA molecules modified on AuNPs form a stem-bulge-stem structure when cocaine exists. The aggregation of AuNPs and color changes of the scattered light in the dark-field image of an LFP were observed. Consequently, the minimal detectable content of cocaine on LFPs was measured down to 90 ng [45].

In addition to the aptasensor based on the passive oligonucleotide-assisted aggregation of AuNPs, the active aggregation of AuNPs, namely, salt-induced self-assembly, was also utilized to establish analytical methods for quantifying cocaine [46–49] and methamphetamine [50]. The strategy is based on the van der Waals attraction between the AuNPs themselves, which induces AuNP self-assembly, and assembly between aptamers and AuNPs, which can prevent the aggregation of AuNPs. In general, the surface of AuNPs was adsorbed with negative ions such as citrate, and they can inhibit the aggregation of AuNPs themselves. However, the addition of salt into the colloid can induce the self-aggregation of AuNPs due to the neutralization of citrate ions on the surface of AuNPs, which reduces the repulsion between AuNPs. This reaction produces the redshift of the absorption wavelength upon SPR, and the color change of the colloid can also be visually observed to change from red to purple. On the other hand, the oligonucleotide can attach to the surface of AuNPs, which creates repulsion between the nanoparticles. Consequently, the absorption wavelength would not transform even in a high salt concentration [42]. According to the theory, Zhang et al. established a colorimetric aptasensor for the detection of cocaine [46]. In the presence of cocaine, the complex, specific secondary structure formed due to the binding of cocaine to the aptamer [51] can resist the attachment of an aptamer onto the surface of AuNPs due to the outer phosphate backbone that can be described as dsDNA, resulting in self-aggregated AuNPs after the addition of salt. In contrast, the aptamer can interact with the surface of AuNPs by van der Waals attraction in the absence of cocaine. Consequently, the self-assembly of AuNPs can be inhibited after the addition of salt into the colloid. Finally, the LOD was 0.6 $\mu\text{g/mL}$ [46]. Attributed to the visual change in the color of the AuNPs, prompt measurements of cocaine relying on RGB color codes by snapping photographs were also developed by Smith et al. and Wang et al. [48,49]. A similar mechanism of the aptasensor can also be fabricated for the detection of methamphetamine in urine samples, and an LOD of 0.12 $\mu\text{g/mL}$ was achieved [50].

3.3. Others

A colorimetric sensor can be developed from the synthesis process of nanoparticles. Amjadi et al. fabricated a biosensor by enhancing the reduction of silver nanoparticles (AgNPs) with the addition of cannabinoids that possess a phenolic group so that they can provide mild reducing properties and

coordinate the reducing agent of AgNO_3 in the process of synthesis of AgNPs. As a result, the increasing SPR absorption peak of AgNPs can be observed, and this phenomenon can be further applied to quantify the species of cannabinoid [52]. Another colorimetric sensor, Au@Ag core-shell nanoparticles, was immobilized with partially corresponding complementary strands of aptamers (as a reporter probe) for the duplexed detection of methamphetamine. The capture probe, with a partially corresponding complementary strand of aptamers, conjugated with MNPs. In the absence of analytes, the reporter probe and capture probe bound to the aptamer and Au@Ag-DNA-MNP complex structures were formed. The intensity of the SPR absorption peak was lower than that in the presence of analytes [53]. A similar mechanism was used to simultaneously duplex the detection of methamphetamine and cocaine by observing multiple dominant wavelengths [54]. The Au@Ag core-shell nanoparticles were synthesized by the shell coating of silver onto the surface of AuNPs, which produced a blueshift of nanoparticles from 520 nm to 400 nm. Moreover, the enhancement of absorption after the synthesis of Au@Ag core-shell nanoparticles was mainly due to surface plasmon damping. Finally, the LODs for methamphetamine and cocaine were measured to be 75 $\mu\text{g}/\text{mL}$ and 1 ng/mL , respectively [54]. In addition to the

application of AgNPs and Au@Ag core-shell nanoparticles for colorimetric sensors, MNPs were also utilized to construct a rapid detection sensor based on a lateral flow strip for cocaine [55]. The principle of the sensor was dependent on the interaction between anti-cocaine antibody-modified MNPs and cocaine, which can influence the further reaction of MNPs to cocaine-BSA and goat anti-mouse IgG antibody immobilized on the surface of the lateral flow strip. After the reaction, two discriminable brown bands can be observed, and the color densities of the bands depend on the cocaine content. Consequently, the quantification of cocaine can be achieved by calculating the ratio of RGB color codes of two bands through a smart phone camera, with an LOD of 5 ng/mL [55]. Similar mechanism of lateral flow assay for cocaine was also conducted by benzoylgonine mAb conjugated AuNPs and a LOQ at 10 ng/mL can be measured in synthetic saliva [56].

The following sensing mechanisms of nanomaterial-based colorimetric sensors are summarized and shown in Fig. 1: (1) ligated-analyte interaction, (2) oligonucleotide-assisted aggregation, (3) salt-induced self-assembly, and (4) others. In colorimetric biosensors, AuNPs are the most widely applied nanomaterials used to perform versatile detection strategies based on surface interactions and optical properties. With the ability to visually

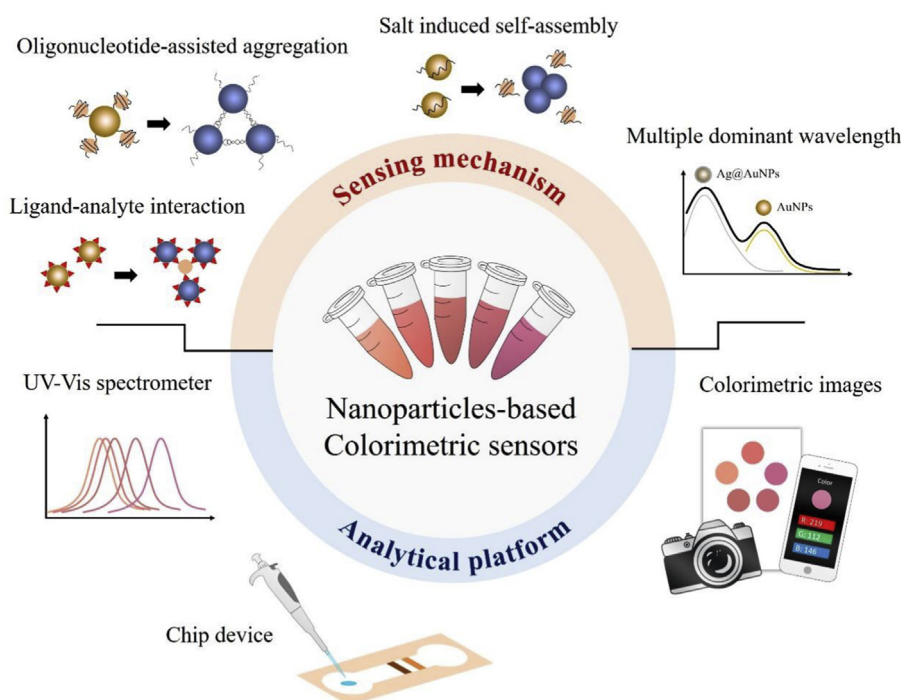


Fig. 1. Colorimetric strategies for illicit drugs based on nanomaterials which combine with versatile analytical platforms.

observe the color change of AuNPs or chromophores, colorimetric methods possess the potential to quickly monitor analytes without dependence on advanced detection instruments. The colorimetric biosensors developed in previous studies are summarized in [Table 3](#) which presents analyte-binding medium, added volume of sample, incubation time, sample matrix and LOD of respective analytical methods. Most colorimetric biosensors can obtain sensitivity values on a scale of $\mu\text{g/mL}$ or ng/mL for analyzing illicit drugs. In addition, a less sample consumption is feasible with the added volume of sample in the range of $1\ \mu\text{L}$ - $1.2\ \text{mL}$ (mostly below $100\ \mu\text{L}$). The recognition of analyte to sensors can be also thoroughly accomplished within 30 min. Some of methods even finished incubation of analyte less than 5 min. For the investigation of prolonged life time of a sensor, a proper storage treatment extended the shelf-life up to 2 months without apparent signal decay [48].

4. Nanomaterial-based fluorescent sensors

Fluorescent detection is regarded as a more sensitive optical sensing technique than the use of a colorimetric sensing system. Conventional fluorescent organic dyes exhibit high sensitivity; however, the disadvantages of fluorescent organic dyes are their high cost and complicated synthesis procedure. In recent years, nanomaterials with fluorescent characteristics, such as NCs, QDs, CDs and UCNPs, have become new alternatives as fluorescent sensors. Several fluorescent sensing mechanisms have also been developed, including specific recognition, fluorescence resonance energy transfer (FRET) and molecular gating. The schematic diagram is shown in [Fig. 2](#). The fluorescent sensors developed in previous studies are summarized in [Table 4](#) which presents analyte-binding medium, added volume of sample, incubation time, sample matrix and LOD of respective analytical methods.

4.1. Noble metal nanomaterial-based sensors

Noble metal nanomaterials with size-dependent optical properties are an alternative to conventional fluorophores or are used as quenchers due to their high quenching ability. There were three applications of noble metal nanomaterials, including stabilizing ligand-induced fluorescent sensors, FRET-based fluorescent sensors and controlled-release fluorescent sensors.

4.1.1. Stabilizing ligand-induced fluorescent sensors

Metal nanoclusters (NCs) were defined as comprising several to a few hundred atoms less than approximately $1\ \text{nm}$ in size. As the metal is on the same scale as the NCs, discrete energy levels can be produced. When the external energy is focused upon the NCs, fluorescence can be induced due to quantum confinement by electronic transitions between discrete energy levels. Compared to conventional organic dyes and semiconductor quantum dots, NCs possess the properties of photostability and low toxicity [16]. In addition, to stabilize the NCs that are prone to self-aggregate, several templates were used to achieve the desired outcome, including molecular ligands [57], dendrimers [58], polymers [59] and DNA [60]. Given the stability and optical properties of NCs, they are suitable for the establishment of biosensors. Furthermore, the NC technique was used to determine the presence of illegal drugs such as cocaine [61–64] and ketamine [65].

In the detection of cocaine, Zhou et al. developed two sensors based on copper nanoclusters (CuNCs) [61] and silver nanoclusters (AgNCs) [62] through the interaction between the NCs and DNA as the template. The nanocluster diameter of Cu can be supported only by double-strand DNA (dsDNA) with an emission wavelength of $596\ \text{nm}$ and an excitation wavelength of $340\ \text{nm}$. According to the specific stabilization of CuNCs by dsDNA, the aptamer can be used as a blocker against the hybridization of DNA by the addition of aptamer-corresponding substances, namely, cocaine, to inhibit the formation of CuNCs. Consequently, the established aptasensor exhibited a detection limit of $30\ \text{ng/mL}$ for cocaine. The DNA sequence with cytosine and guanine provides an ideal scaffold for the synthesis of AgNCs due to the strong affinity for silver ions. Moreover, the emitted fluorescence of AgNCs can be enhanced through close proximity to a guanine-rich DNA sequence because guanine possesses the lowest oxidation potential among nucleotides and can play the role of an electron donor to reduce the oxidized NCs to emit unoxidized NCs [66]. According to the theory of fluorescence-enhanced NCs, Zhou et al. also established an aptasensor based on AgNCs for the detection of cocaine [62]. The two oligonucleotides were designed for the synthesis of AgNCs with guanine-rich sequences, and they can hybridize together to form a specific secondary structure only in the

Table 3. Various nanomaterial-based colorimetric sensors for analysis of illicit drugs.

Nanomaterial-based colorimetric sensors	Sample volume	Incubation time ¹	Sample	Limit of detection	Ref.
Small molecular-based AuNP sensors					
Citrate-capped AuNPs	1 mL	-	Bone Bone marrow Soil	0.62 µg/mL for codeine sulfate	[34]
Citrate-capped AuNPs	1.2 mL	10 min	Urine	0.3 µg/mL for codeine 0.3 µg/mL for methadone 0.29 µg/mL for morphine 6.7 µg/mL for noroxycodone 0.31 µg/mL for thebaine	[35]
Citrate-capped AuNPs	-	10 min	Serum	0.15 µg/mL for morphine	[36]
Melamine-modified AuNPs	-	3 min	Urine Blood	0.28 ng/mL for clonazepam	[40]
Melamine-modified AuNPs	-	10 min	Bone Bone marrow Serum Urine	2.7 ng/mL for codeine 4.9 ng/mL for morphine	[41]
Aptamer-based AuNP sensors					
(A) Oligonucleotide-assisted aggregation					
Complementary strand-modified AuNPs and cocaine aptamer Aptamer sequence: 5'-ACTCATCTGTGAA TCTCGGGAGACAAGG ATAAATCCTTCAATGA AGTGGGTCTCCC-3'	-	10 s	-	No LOD (for cocaine)	[44]
Cocaine aptamer fragment 1-modified AuNPs and cocaine aptamer fragment 2-modified AuNPs Aptamer sequence (fragment 1): 5'- GTTCTTCAATGAAG TGGGACGACATTT TTTTTTT-SH-3' Aptamer sequence (fragment 2): 5'- GGGAGTCAAGAAC TTTTTTTTT-SH-3'	10 µL	30 min	Fingerprints	90 ng for cocaine	[45]
(B) Salt-induced self-assembly					
AuNPs and cocaine aptamer fragment 1 & 2 Aptamer sequence (fragment 1): 5'- GTTCTTCAATGAAGT GGGACGACA-3' Aptamer sequence (fragment 2): 5'- GGGAGTCAAGAAC-3'	2 µL	2-3 min	-	0.6 µg/mL for cocaine	[46]
AuNPs and cocaine aptamer	20 µL	30 min	Urine	0.3 ng/mL for cocaine	[47]

(continued on next page)

Table 3. (continued)

Nanomaterial-based colorimetric sensors	Sample volume	Incubation time ¹	Sample	Limit of detection	Ref.
Aptamer sequence: 5'-GGGAGACAAGG AAAATCCTTCAATGAA GTGGGTCGACA-3' AuNPs and cocaine aptamer	18.2 µL	30 min	-	0.25 mg/mL for cocaine	[48]
Aptamer sequence: 5'- GGCGACAAGGAAAATC CTTCAACGAAGTGGGT CGCC-3' AuNPs and cocaine aptamer fragment 1 & 2	1 µL	5 min	-	2.36 µg for cocaine	[49]
Aptamer sequence (fragment 1): 5'-ACAGCAGGTGAAGT AACTTCTTG-3' Aptamer sequence (fragment 2): 5'- GGGAGTCAAGAAC-3' AuNPs and methamphetamine aptamer	120 µL	5 min	Urine	0.12 µg/mL for methamphetamine	[50]
Aptamer sequence: 5'-ACGGTTGCAAGTGGG ACTCTGGTAGGCTGGGT TAATTTGG-3'					
Others					
AgNPs	-	30 min	Hashish	52 ng/mL for cannabidiol 77 ng/mL for cannabinol 65 ng/mL for tetrahydro- cannabinol	[52]
Complementary strand- modified Au@AgNPs and methamphetamine/cocaine aptamer	10 µL	-	Urine	15 pg/mL for methamph- etamine	[53]
Aptamer sequence (methamphetamine): 5' -ACGGTTGCAAGTGGGA CTCTGGTAGGCTGGGTA ATTTGG-3' Aptamer sequence (cocaine): 5'-GGGAGACAAGGATAA ATCCTTCAATGAAGT GGTTCGATA-3'				0.15 ng/mL for cocaine	
Complementary strand (methamphetamine)-modified Au@AgNPs and methamphetamine aptamer	5 µL	30 min	Waste water	75 pg/mL for methamphetamine	[54]
Complementary strand (cocaine)-modified AuNPs and cocaine aptamer				1 ng/mL for cocaine	
Aptamer sequence (methamphetamine): 5'-ACGGTTGCAAGTG GGACTCTGGTAGGCT GGTAAATTTGG-3' Aptamer sequence (cocaine): 5'-GGGAGACAAGGATAA ATCCTTCAATGAAG TGGGTCGATA-3'					

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Table 3. (continued)

Nanomaterial-based colorimetric sensors	Sample volume	Incubation time ¹	Sample	Limit of detection	Ref.
Cocaine antibody-modified MNPs	80 μ L	10 min	Urine	5 ng/mL for cocaine	[55]
Benzoylcegonine mAb conjugated AuNPs	100 μ L	-	Synthetic saliva	10 ng/mL for cocaine	[56]

Abbreviation: AuNPs: gold nanoparticles; AgNPs: silver nanoparticles; Au@AgNPs: gold-silver core-shell nanoparticles.

¹ Incubation time: the time of recognition of the analyte in sensing procedure.

presence of cocaine. Finally, the LOD of cocaine was 30 ng/mL.

Other aptasensors based on AgNCs were also developed. For instance, Zhang et al. established an aptasensor in combination with a nicking endonuclease-assisted signal amplification method for the detection of cocaine in serum samples with an LOD of 0.6 ng/mL [63], Sharon et al. also fabricated an aptasensor based on FRET between AgNCs and quenchers with an LOD of 91 ng/mL [64], and Ding et al. used a DNA sequence (dC12) composed of an AgNC template and ketamine-binding DNA as the scaffold for the stabilization of AgNCs. In the presence of ketamine, the DNA scaffold of the AgNCs disintegrated and further interacted with ketamine, resulting in the transformation of the DNA complex structure so that the fluorescence emitted from the AgNCs could be quenched. The LOD was 60 pg/mL [65]. A novel sensing system based on AgNCs and the technique of artificial intelligence was established for the detection of illegal drugs [67]. The sensing principle is mainly based on the change in

the fluorescence of AgNCs influenced by the interaction between the analyte and AgNCs. After that, sensing statistics can be integrated by a deep learning (DL) model, which is a subfield of artificial intelligence. The DL model can be utilized to construct three-dimensional fingerprint-like spectra. The spectra are composed of recognizable peak distributions by a fluorescence excitation emission matrix while the analyte interacted with AgNCs. In this study, the spectra for illicit drugs, namely, 3,4-methylenedioxyamphetamine (MDA), MDMA, codeine, meperidine and methcathinone, were established. The novel detection technique was capable of identifying and semiquantifying these drugs down to 2 μ g/mL and possessed the potential to rapidly identify multiple illicit drugs [67].

4.1.2. FRET-based fluorescent sensors

The typical principle of fluorescent sensors is mainly based on the quenching effect of the fluorophore by FRET. The excited-state energy from the

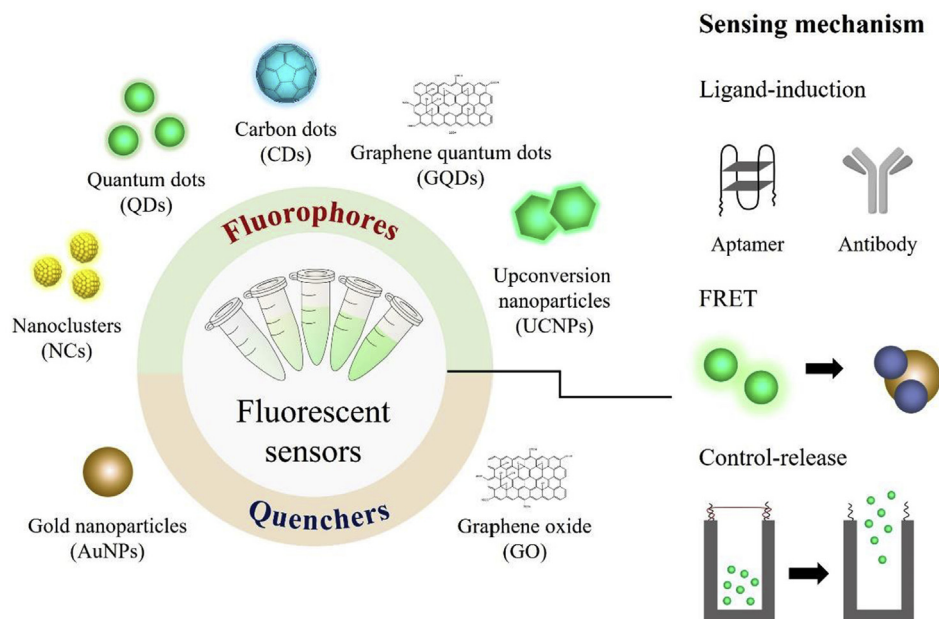


Fig. 2. Fluorometric strategies for illicit drugs based on nanomaterials which were constructed as fluorophore or quencher and utilized to establish diverse sensing mechanisms.

Table 4. Various nanomaterial-based fluorescent sensors for analysis of illicit drugs.

Nanomaterial-based fluorescent sensors	Sample volume	Incubation time ¹	Sample	Limit of detection	Ref
Noble metal nanomaterials-based sensors					
(A) Salt-induced self-assembly					
DNA-CuNCs and cocaine aptamer Aptamer sequence: 5'-GACAAGGAA AATCCTTCA ATGAAGTGGGTC-3'	-	15 min	-	30 ng/mL for cocaine	[61]
DNA-AgNCs and cocaine aptamer fragment 1 & 2 Aptamer sequence (fragment 1): 5'- TTCGTTCTTCAAT GAAGTGGGAC GACAATGTGGAG GGT-3' Aptamer sequence (fragment 2): 5'- AGGGACGG GAAGGGAGTCAA GAACGAA-3'	-	15 min	-	30 ng/mL for cocaine	[62]
DNA-AgNCs and cocaine aptamer Aptamer sequence: 5'-CCACTGACCTC AGCATGTCGAGGG AGACAAGGAAAAT CCTTCAATGAAGT GGGTCGACATG CTGA-3'	5 µL	1 h	Serum	0.6 ng/mL for cocaine	[63]
DNA-AgNCs and cocaine aptamer Aptamer sequence: 5'-GCTGCAGAAATGG GATCTTCATGACA AGGAAAATCCTTC AATGAAGTGGGTC AATTAT-3'	-	30 min	-	91 ng/mL for cocaine	[64]
DNA-AgNCs and ketamine aptamer Aptamer sequence: 5'-TGGGGATGGAG AACTCCCCCCCC CCCC-3'	30 µL	5 min	Blood	60 pg/mL for ketamine	[65]
AgNCs	-	3 min	Urine	No LOD for MDA, MDMA, codeine, meperidine, methcathinone	[67]
(B) FRET-based fluorescent sensors					
Cocaine aptamer-modified AuNPs and complementary strand-modified SNPs	10 µL	40 min	Serum	89 pg/mL for cocaine	[72]

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Table 4. (continued)

Nanomaterial-based fluorescent sensors	Sample volume	Incubation time ¹	Sample	Limit of detection	Ref
Aptamer sequence: 5'-CCATAGGGAGAC AAGGATAAATCC TTCAATGAAGTGGG TCTCCC-SH-3' Complementary strand-modified AuNPs and cocaine aptamer	3 μ L	1 h	-	No LOD for cocaine	[73]
Aptamer sequence (cocaine): 5'-Cy5-AAGTGGGG AGACAAGGATAA ATCCTTCAATGAAG TGGGTCTCCC-3'	5 μ L	4 h	-	9.1 ng/mL for cocaine	[74]
Cocaine aptamer and AuNPs	-	3 min	Serum Urine	19 pg/mL (serum) for morphine 17 pg/mL (urine) for morphine	[75]
Aptamer sequence (cocaine aptamer fragment 1): 5'-AMCA-AGACAAG GAAAA-3' Aptamer sequence (cocaine aptamer fragment 2): 5'-TCCTTCAATG AAGTGGGTCG-3'	29 _{equivalents}	5 min	-	No LOD for methamphetamine	[76]
NTS@SNPs	80 μ L	25 min	Serum	25 pg/mL for cocaine	[77]
Cocaine aptamer fragment 1-modified SNPs and cocaine aptamer fragment 2 Aptamer sequence (fragment 1): 5'-biotin- GGGAGTCAAGAAC- BHQ-1-3' Aptamer sequence (fragment 2): 5'-FAM- GTTCTTCAATGAAGT GTGGGACGACA- TAMRA-3'	(C) Control-released fluorescent sensors				
Pseudorotaxane capped mesoporous SNPs	100 μ L	2 h	Water	0.94 μ g/mL for MDMA	[79]
complementary strand-modified NAA and cocaine aptamer	100 μ L	20 min	Saliva	0.15 μ g/mL for cocaine	[80]

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Table 4. (continued)

Nanomaterial-based fluorescent sensors	Sample volume	Incubation time ¹	Sample	Limit of detection	Ref
Aptamer sequence: 5'-TTTTGGGGG GGGGAGACAAG GAAAATCCTTCAA TGAAGTGGGT CTCCAGGGGGG TTTT-3'					
Quantum dots-based fluorescent sensors					
morphine antibody-labeled CdS@MAA-QDs	0.2 µL	-	-	No LOD for morphine	[82]
Morphine antibody-labeled CdSe/ZnS QDs	100 µL	-	Soup	0.27 ng/mL for morphine	[83]
7-aminoclonazepam antibody-modified CdTe-QDs	-	15 min	Urine	21 pg/mL for 7-aminoclonazepam	[84]
Complementary strand-modified QDs and cocaine aptamer	-	-	-	0.15 µg/mL for cocaine	[85]
Aptamer sequence: 5'-ACTCATCTGT GATATCTCGGGAGA CAAGGAAAATCCTTC AATGAAGTGGGT CTCCC-3'					
Complementary strand-modified QDs and cocaine aptamer	80 µL	5 min	-	36 µg/mL for cocaine	[86]
Aptamer sequence: 5'-ACTCATCTGTGAAT CTCGGGAGACAAG GATAAATCCTTCAAT GAAGTGGGTCT CCC-3'					
AuNPs-conjugated cocaine aptamer-modified QDs	25 µL	3 h	Artificial urine	40 pg/mL for cocaine	[87]
Aptamer sequence: 5'-C ₆ -NH ₂ -AGAC AAGGAAAATCC TTCAATGAAGT GGGTCG-SH ₂ -C ₃ -3'					
L-cysteine capped CdS QDs	-	-	Urine	1.8 ng/mL for methamphetamine (fluorescence) 0.086 ng/mL for methamphetamine (chemiluminescence)	[88]
D-Cysteine molecules-functionalized CdSe QDs	-	-	-	17 ng/mL for L-morphine	[89]
Streptavidin-QDs, complementary strand-modified AuNPs and cocaine aptamer	10 µL	25 min	-	0.15 pg/mL for cocaine	[90]
Aptamer sequence: 5'-ATCTCGGGAGAC AAGGATAAATCC TTCAATGAAGTGGG TCTCCCAAAAAAAAAA AA-Biotin-3'					

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Table 4. (continued)

Nanomaterial-based fluorescent sensors	Sample volume	Incubation time ¹	Sample	Limit of detection	Ref
Carbon nanomaterials-based fluorescent sensors					
Methamphetamine aptamer-modified CDs and CoOOH nanosheets Aptamer sequence: 5'-NH ₂ -(CH ₂) ₆ -ACGGTTGCAAGTGGACTCTG GTA GGCTGGGTTAAT TTGG-3'	-	20 min		0.48 ng/mL for methamphetamine	[92]
CDs	1.5 mL	5 min	Beverage	2.0 µg/mL for nitrazepam	[93]
CDs-functionalized paper	10 µL	10 min	Urine	1.3 µg/mL for 4-chloroethcathinone	[94]
GQDs	-	1 min	-	1.48 µg/mL for methamphetamine 0.5 µg/mL for morphine	[97]
GQDs with antimorphine (antibody)	-	-	-	18 ng/mL for morphine	[98]
GO and cocaine aptamer fragment 1 & 2 Aptamer sequence (cocaine aptamer fragment 1): 5'-GGGAGTCTCAAG AAC-FAM-3' Aptamer sequence (cocaine aptamer fragment 2): 5'-GTTCTTCAATGAAG TGGGACGACTAT-3'	-	10 min	Plasma	30 pg/mL for cocaine	[101]
GO and cocaine aptamer Aptamer sequence: 5'-GGGAGACAAGGAA AATCCTTCAATGAAG TGGGTCTCCCTAGTT TTCTAGGGAGAC-PO ₄ -3'	20 µL	20 min	Urine	57 ng/mL for cocaine	[102]
Cocaine aptamer fragment 1-modified GQDs and cocaine aptamer fragment 2-modified AuNPs Aptamer sequence (fragment 1): 5'-NH ₂ -(CH ₂) ₆ -TTTTGGGAGTCA AGAACGAA-3' Aptamer sequence (fragment 2): 5'-SH-(CH ₂) ₆ -TTCGTTCTTCAATG AAGTGGGACGA CA-3'	1 µL	1 h	Plasma	30 ng/mL for cocaine	[103]
			Serum		
			Saliva		
			Urine		

(continued on next page)

Table 4. (continued)

Nanomaterial-based fluorescent sensors	Sample volume	Incubation time ¹	Sample	Limit of detection	Ref
Upconversion nanoparticles-based fluorescent sensors					
Cocaine aptamer fragment-modified AuNPs and UCNPs Aptamer sequence: 5'-SH-TTTTTACAGC AGGGTGAAGTAAC TTCTTG-3'	2 μ L	40 min	Rat plasma	LOQ: 3 ng/mL (aqueous solution) for cocaine	[105]
			Saliva	LOQ: 15 ng/mL (saliva) for cocaine	
Cocaine aptamer-modified UCNPs Aptamer sequence: 5'-NH ₂ -TTTTTGGACAA GGAAAATCCTTCAAT GAAGTGGGTC-3'	0.1-10 μ g	30 min	Fingerprints	0.1 μ g for cocaine	[106]

Abbreviation: CuNCs: copper nanoclusters; AgNCs: silver nanoclusters; MDA: 4,5-methylene-dioxy amphetamine; MDMA: 3,4-methylene dioxy methamphetamine; SNPs: silica nanoparticles; NTS: 4-thiophene-N-propyl(trithoxysilane)1,8-naphthalimide; NAA: nanoporous anodic alumina; MAA: mercaptoacetic acid; CDs: carbon dots; CoOOH: cobalt oxyhydroxide; GQDs: graphene quantum dots; GO: graphene oxide; UCNPs: upconversion nanoparticles.

¹ Incubation time: the time of recognition of the analyte in sensing procedure.

fluorophore as a donor transfers to the quencher as an acceptor-based dipole-dipole interaction in the context of the proximity between the donor and acceptor in the range from 10 to 100 Å [68]. Furthermore, alternatives to quenchers, such as metal nanoparticles (AuNPs) and graphene oxide, are based on the properties of surface plasmon resonance (SPR) and heterogeneous electronic structures [69]. The heterogeneous electronic structure of graphene oxide is attributed to its composition of sp² and sp³ binding, which provides properties of FRET and nonradiative dipole-dipole coupling [69,70].

Sensors coupled with aptamers, known as aptasensors, have been developed to enhance detection selectivity. The first fluorescent aptasensor aimed at detecting cocaine was established by Stojanovic et al. [71]. The strategy of detection was based on molecular beacons that were labeled with fluorescein as the fluorophore and dabcyI as the quencher on the double end of the cocaine-specific aptamer. The aptamer can form a secondary structure after the presence of cocaine. The conformational change of the aptamer shortens the proximity between the fluorophore and the quencher, which produces fluorescent degeneration.

Gold nanoparticles (AuNPs) are ideal candidates for fluorescent quenchers with unique optical properties by surface plasmon resonance (SPR) [72–75]. The aptasensor coupled with AuNPs can be divided into unmodified and oligonucleotide-modified. For instance, Zhang et al. developed an aptasensor based on complementary aptamer-modified AuNPs for the detection of cocaine [73].

The interaction between the cocaine and the fluorescent aptamer allows the aptamer to exhibit steric hindrance by forming a secondary structure with cocaine. As a result, the prehybridized fluorescent aptamer can be released, and the fluorescence can be recovered. Luo et al. developed an aptasensor based on unmodified AuNPs for the detection of cocaine [74]. The fluorescent aptamer can attach onto the surface of AuNPs with van der Waals forces, and the fluorescence will be quenched due to the close distance between the aptamer and AuNPs. In the presence of cocaine, the complex of the aptamer and cocaine becomes a secondary structure that resists the attachment to AuNPs by electrostatic repulsion [42] and allows the recovery of fluorescence. Consequently, the LOD for the detection of cocaine was 9.1 ng/mL. Another fluorescent biosensor was also developed by the direct interaction between the analyte and AuNPs. Nebu et al. established a biosensor for the detection of morphine based on the competitive attachment between morphine and fluorescein onto the surface of AuNPs to influence the quenching of fluorescein by AuNPs, and this sensor had an LOD up to 17 pg/mL for urine and 19 pg/mL for serum [75].

A similar mechanism of aptasensors coupled with silica nanoparticles (SNPs) was applied for signal amplification [72,76,77]. Sarreshtehdar et al. reported an aptasensor based on AuNPs as the quencher and SNPs for the enhancement of fluorescent intensity, and the technique possessed high sensitivity, up to 89 pg/mL, for the detection of cocaine in serum [72]. Rouhani reported a nanosensor based on 1,8-naphthalimide-thiophene-

doped SNPs for the detection of methamphetamine. The interaction between 1,8-naphthalimide and methamphetamine not only triggers the exhibition of fluorescence but also enhances the sensitivity [76]; Abnous et al. also established an aptasensor based on SNPs for the detection of cocaine in serum with a limit of detection of 25 pg/mL [77].

4.1.3. Control-released fluorescent sensors

In addition to nanomaterials that possess optical properties to develop sensor systems, porous nanomaterials can also be utilized to construct a detection system on the basis of a molecule gate that can efficiently control the release of molecules inside the cavities of porous nanomaterials. Mesoporous silica nanoparticles (SNPs) were used to establish a sensing platform for the detection of illicit drugs. Mesoporous SNPs have many cavities on the surface, and they possess a large load capacity, biocompatibility and on-command delivery application [78]. The fundamental principle of fluorescent controlled-released SNPs is accomplished by capping the cavities by molecules and oligonucleotides to prevent the release of fluorophores in the cavities. As the analytes interact with the capping substances, the gate can be destroyed, and the fluorophores can be released. With this theory, pseudorotaxane capped mesoporous SNPs were established by Lozano-Torres et al. to detect MDMA. Detection can be accomplished depending on the competitive interaction between MDMA and pseudorotaxane, which induces the uncapping of cavities and facilitates the release of fluorescein. Consequently, an LOD of 0.94 $\mu\text{g/mL}$ could be achieved for MDMA [79]. In addition, alumina can also be constructed as nanoporous anodic alumina (NAA), which is capable of loading small molecules. Ribes et al. fabricated an aptasensor based on NAA for cocaine that possesses cavities with an average size of 8 nm [80]. Likewise, the assistance of the cocaine-aptamer complex provided a molecular gate that blocked the release of fluorescent reporters, rhodamine B, keeping them in the cavities. In the presence of cocaine, the aptamer bound with cocaine and detached from the NAA. Subsequently, rhodamine B be released from of cavities. Consequently, the quantification of cocaine can be achieved, and the LOD for cocaine was 151 ng/mL in saliva [80].

4.2. Quantum dot-based fluorescent sensors

Quantum dots (QDs) are nanocrystals composed of semiconducting material with a small size, mainly in the range of 2–10 nm. The diameters of QDs are

intermediate between the bulk of semiconductors and discrete molecules. Attributed to the tiny size of QDs in close proximity to the wavelength of the electron, the phenomenon of quantum confinement effects is due to the energy gap between the valence band and the conducting band. The size-dependent band gap provides the optical and electronic properties of QDs, such as excitation and electron-hole interactions, which lead to photoluminescence [17,81]. With the property of fluorescent exhibition, QDs have been used in the development of many sensors for the detection of various substances in a wide variety of industries, such as the environment, biology, and medicine. Moreover, QD techniques in combination with other techniques, such as immunoassays [82–84] and aptamers [85–87], have also been used to detect illegal drugs in recent research, and these techniques are considered reliable and useful tools for the establishment of trace analytical methods.

In the development of sensors simply based on the modification of QDs, Hassanzadeh et al. developed a sensor based on L-cysteine capped CdS QDs for the detection of methamphetamine. The interaction of methamphetamine to the surface of the QDs, which can affect the efficiency of fluorescent emission and an LOD of 1.8 ng/mL, can be obtained in a urine sample [88]. Similarly, the sensor based on D-cysteine-functionalized CdSe possessed the selectivity of chiral analyte on the detection of L-morphine with the LOD at 17 ng/mL [89]. Furthermore, the surfaces of QDs modified with an anti-morphine antibody and denatured bovine serum albumin were also established as immunosensors for the detection of morphine [82,83] and 7-aminoclonazepam [84].

Aptasensors coupled with QDs were also utilized to detect cocaine. Two aptasensors, one based on QDs and Cy5 and the other based on QDs, Cy5 and Iowa Black RQ, were established through the mechanism of FRET for the detection of cocaine [85]. In the aptasensor based on QDs and Cy5, the QD surface was modified with a short sequence of oligonucleotides that can hybridize with the cocaine aptamer, and Cy5 was modified on another partly complementary sequence of the cocaine aptamer. The Cy5-modified complementary sequence of cocaine aptamer can hybridize with the cocaine aptamer, and the mechanism of FRET was further instigated by the energy transfer from the QDs to Cy5 with an excitation wavelength at 488 nm in the absence of cocaine. After the addition of cocaine, the aptamer can form a specific secondary structure that resists hybridization between the cocaine aptamer and the Cy5-modified complementary aptamer.

Therefore, FRET cannot be induced, and the emission signal of QDs at 605 nm can be observed. Finally, the aptasensor had a detection limit of 0.15 $\mu\text{g/mL}$. The CdSe/ZnS core-shell QDs were used as the fluorophore and AuNPs were used as the quencher for the detection of cocaine and benzoylecgonine. The analytical method successfully quantified the analytes with an LOD of 41 pg/mL for cocaine and 0.48 $\mu\text{g/mL}$ for benzoylecgonine in artificial urine [87]. In addition, the technique in combination with QDs, aptamers and AuNPs was also developed by Zhang et al. The aptamer-modified microfluidic beads served as the main body of the sensing platform [90]. Complementary-aptamer DNA-AuNPs (cDNA-AuNPs) loaded with horseradish peroxidase (HRP) were used as the medium to trigger the interaction between tyramine-biotin and streptavidin-QDs. The linkage of biotin-streptavidin provided strong fluorescence to microbeads due to the numerous QDs bound to them. However, the interaction failed to function properly in the presence of cocaine because cocaine can occupy the hybridized sites of the cDNA-AuNPs to microbeads so that further reaction will be interrupted. Finally, an LOD of 0.15 pg/mL could be achieved for cocaine through this method [90].

4.3. Carbon nanomaterial-based fluorescent sensors

The development of carbon nanomaterials has drawn great attention to the application of sensing systems as they have less toxicity and environmental hazards than QDs. Carbon nanomaterials that are widely used in the establishment of biosensors can be divided into three parts: carbon dots (CDs), graphene quantum dots (GQDs) and graphene oxide (GO).

Quantum-sized carbon nanoparticles, known as CDs, possess the stable property of photoluminescence. The principle of photoluminescence from CDs may be caused by the presence of surface energy traps that become emissive upon stabilization because of surface passivation [18,91]. Saberi et al. developed an aptasensor using CDs as the fluorophore and cobalt oxyhydroxide nanosheets (CoOOH) as the quencher for the detection of methamphetamine and a schematic illustration of the aptasensor [92]. The CDs were synthesized from the grape leaves by hydrothermal treatment and were further immobilized onto the aptamer of methamphetamine. The CD-modified aptamer can attach onto the surface of the CoOOH nanosheet by van der Waals forces in the absence of methamphetamine, and the fluorescence emitted from the CDs was quenched by CoOOH through FRET. In

contrast, the aptamer can conjugate with methamphetamine, and the complex can resist the interaction between the aptamer and the CoOOH nanosheet. Consequently, fluorescence can be observed, and the limit of detection of methamphetamine was measured to be 0.48 ng/mL in human plasma. Furthermore, the fluorescence emitted from CDs can also be quenched according to the absorption of the target onto the surface of CDs. The attachment of the target to CDs triggers electron transfer, which depends on the functional groups of the analyte, and further FRET occurs. Yen et al. developed a biosensor based on CDs for the detection of nitro-containing benzodiazepines, namely, nimetazepam, which is regarded as a type of date rape drug. This method provides an LOD for nimetazepam at 2.13 $\mu\text{g/mL}$ in beverages such as beer, juice, wine and whiskey [93]. Likewise, CDs were also modified onto paper for the detection of 4-chloroethcathinone and a LOD can be obtained to be 1.3 $\mu\text{g/mL}$ in urine sample [94].

Similar to the CDs, GQDs also possess the optical property of photoluminescence with significant quantum confinement and edge effects as the size of GQDs is below 100 nm [95,96]. Different from the spherical nanoparticles of CDs composed of sp^3 hybridized carbon, the GQDs are composed of sp^2 hybridized carbon, which represents a layer of crystalline structure. A sensor based on GQDs was designed for the detection of D -methamphetamine and L -morphine through their interaction with GQDs. The quenching effect was observed by the addition of methamphetamine. Meanwhile, the fluorescence enhancement effect was found by the addition of morphine. The limits of detection for D -methamphetamine and L -morphine were 1.48 $\mu\text{g/mL}$ and 0.5 $\mu\text{g/mL}$, respectively [97]. Furthermore, the LOD of morphine was improved to 18 ng/mL by using GQDs modified with antimorphine [98].

Apart from quantum dot-characterized carbon materials, another widely applied technique is graphene oxide (GO), which is a thin sheet of graphite fabricated by “top-down [99]” or “bottom-up [100]” methods. GO possesses the property of quenching the fluorescent species by FRET or nonradiative dipole-dipole coupling as the distance between the GO and fluorophore is less than approximately 20 nm. Moreover, the ionic groups and aromatic groups of GO allow charged species such as proteins and DNA to attach onto the GO surface by electrostatic interactions and π - π stacking, respectively [69]. Consequently, GO can easily capture fluorescent substances to produce quenching effects. GO was used in the development of a biosensor for the detection of cocaine in body fluids,

namely, urine, plasma, serum and saliva [101–103]. Zhang et al. established an aptasensor based on GO as the quencher and exonuclease III (Exo III) for signal amplification [101]. Exo III was a crucial factor in the feasibility of the aptasensor, which possessed the property of cleaving the 3-hydroxyl termini of mononucleotides from double-stranded DNA and acted from the 3' to 5' direction [104]. In the presence of cocaine, the aptamer can bind with the cocaine and form a specific secondary structure. Subsequently, the partly complementary DNA sequence corresponding to the aptamer can be further hybridized with the folding structure to form double-stranded DNA. The addition of Exo III can cleave the complementary DNA modified with FAM into mononucleotides. Therefore, FAM failed to attach to the surface of GO, and fluorescence was observed. On the other hand, the complementary DNA can attach onto the surface of GO in the absence of cocaine, and the quenching of fluorescence was achieved. The biosensor was established with an LOD of 30 pg/mL in the plasma sample.

4.4. Upconversion nanoparticle-based fluorescent sensors

In recent years, nanomaterials constructed by rare earth elements such as yttrium (Y), ytterbium (Yb) and erbium (Er), namely, upconversion nanoparticles (UCNPs), have been utilized as biosensors. Attributed to the composition of rare earth elements, UCNPs possess the unique trait of emitting ultraviolet/visible (UV/Vis) light under near-infrared excitation, which efficiently circumvents interference. This property is achieved through intraconfigurational transitions by rare earth elements with abundant energy levels that allow continuous energy transition from low level excitation to high level emission [19]. In addition, the surface of UCNPs is compatible with modifying substances such as oligonucleotides and polymers. He et al. constructed a portable UCNP-based paper device coupled with aptamer-modified AuNPs for the prompt detection of cocaine free from the laboratory. The cellulose filter paper device was immobilized with PEI-UCNPs and NH₂-anti-cocaine aptamer fragments. Another fragment of anti-cocaine aptamers was modified onto AuNPs, which acted as a quencher to diminish the luminescence of UCNPs. In the presence of cocaine, two aptamer fragments can link together and shorten the distance between AuNPs and UCNPs. As a result, the luminescence can be quenched, and cocaine quantification can be accomplished with LOQs of 3 ng/mL and 15 ng/mL in aqueous solution

and saliva, respectively [105]. In addition, UCNPs were also used for LFP detection. Wang et al. developed an aptasensor based on aptamer-modeled UCNPs as signal reporters of LFP for the detection of cocaine, and the method was able to be used to monitor the content of cocaine down to 0.1 µg [106].

In summary of nanomaterial-based fluorescent sensors, the utilization of nanomaterials in an analytical method provides superior detection efficiency for monitoring illicit drugs. LODs of analytes can be measured down to the range of pg/mL and ng/mL. Furthermore, less sample consumption of approximately 100 µL can be also obtained in most established methods. For incubation time of analyte to sensor, some methods can accomplish the reaction within 10 min which achieve the strategy of rapid detection.

5. Conclusion

Attributed to the development of analytical strategies coupled with nanomaterials, features of prompt monitoring, high sensitivity, economical equipment and simple manipulation can be acquired. These advantages provide efficient detection techniques for illicit drugs in bodily fluids and the environment. This review summarizes the application of nanomaterials with respect to the establishment of analytical methods divided into sample pretreatment, colorimetric and fluorescent sensors. Sample pretreatment methods using metal magnetic nanoparticles offer high extraction efficiency with short-term consumption and target specificity, which is more straightforward than traditional sample preparation methods. Colorimetric methods were mainly based on the unique optical properties of AuNPs and AgNPs with representative extinction wavelengths that can change following their aggregation. Fluorescent sensors were also successfully developed by the assistance of fluorophores, namely, NCs, QDs, CDs, UCNPs and quenchers such as AuNPs, CNTs and GO. In addition to these detection strategies, nanomaterials can also be utilized to analytical methods based on surface enhanced raman scattering (SERS) for illicit drugs which were investigated in other literature [107,108]. With the application of nanomaterials for illicit drugs, numerous innovative methods can be constructed in combination with other techniques, such as antibodies, aptamers, MIPs, chip (paper) devices and artificial intelligence. Some of these methods even provide high sensitivity up to pg/mL, similar to the performance of conventional sophisticated instruments. Among these detection methods for

illicit drugs, many of them were combined with aptamers, which possess high compatibility with nanomaterials and can be utilized to improve specificity. However, aptamers for illicit drugs have not been sufficiently established because the majority of analytical methods with the assistance of aptamers were developed for cocaine and methamphetamine, while a minority were developed for codeine and ketamine. Aptamers corresponding to other illegal drugs remain incompletely developed, especially for those that have been prevalent in recent years, such as cannabis and morphine. The establishment of analytical methods coupled with aptamers is still considered a potential approach to facilitate the monitoring of a wide variety of forensic drugs. Although the clinical detection of forensic drugs currently relies on immunoassays and sophisticated instruments such as HPLC-MS and GC-MS, novel biosensors in combination with nanotechnology are expected to realistically monitor forensic drugs in the future.

Conflict of interest

The authors have declared no conflict of interest.

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